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MOX based E- Nose for Non-Invasive Biomedical Applications

Abstract. The non-invasive method to diagnosis any disease is an attractive topic of research due to its rapid, cost effective, convenient and efficient technique. The Health status of a patient can be directly known by examined of volatile organic compound (VOC) of a patient, and this VOC can be studied by an electronic nose (e-nose). E- Nose can be easily detect different types of diseases such as lung cancer, diabetics, by analyzing the exhaled breath of a patient. In the proposed work, a brief overview has been provided about different techniques used to develop the E-nose. The importance of Low temperature co-fired ceramics (LTCC) based breath analyzer and future objectives has discussed.

Streszczenie. EW artykule przedstawiono koncepcję wykorzystania analizatora zapachów tzw. E-nosa do wykrywania chorób na podstaiw badania wydychanego powietrza. Przedstawiono różne techniki analizy. Szczególną uwagę poświecono czujnikowi typu LTCC. (Wykorzystanie analizy wydychango powietrza do wykrywania chorób).

Keywords: LTCC, volatile organic compound, Biomarker, sensor, metal oxide MOX sensor. Słowa kluczowe: sztuczny nos – E-nos, analiza wydychango powitrza

Introduction

In the modern world, the different types of devices and equipment have been used to diagnosis human diseases [1]. Therefore, health care technology becomes the focal point of the researcher, which is an interesting research topic in biomedical engineering. Breathe odours becoming a convenient and efficient technique. Due to its extensive advantages over urine analysis and blood testing, it shows considerable thinking for researchers. It has low complexity than other tests and responsible to complete analysis of all the compounds present. It provides detail about respiratory functions with low complexity. Breath analysis can be applied to detect disease through the detection of VOC produced by the human breath such as ammonia, acetone, nitric oxide, ethanol, carbon dioxide, etc. These VOCs have different concentrations for different types of compounds for a healthy human breath and a sick human breath. For example, if concentration of acetone and ethanol vapors is high in breath which indicates metabolic products is more in the bloodstream, which leads obesity in a patient. Similarly if ammonia vapor found in the breath of patients which is a product of protein and nucleic metabolism which indicates that patients have renal diseases [2]. Therefore, analysis of different exhaled VOCs is helpful in detection of various diseases [3]. Breath analysis shows a potential tool for noninvasive, real-time illnesses diagnostics, metabolic status monitoring, and drug monitoring [4]. It is probably for early detection of an early stage of lung cancer, liver diseases, asthma, diabetes, etc [5, 6]. The breath test over conventional laboratory tests is non-invasive, safe, and painless. The breath analysis system developed using an electronic nose (e-nose) is rapid, inexpensive, more flexible than a urine analysis, and more comfortable than a blood analysis. The figure 1 indicates some major diseases which are related with concentration of different VOCs.

The analysis of breath can be done by an Electronic nose (E-nose). An Electronic nose (E-nose) is used to discriminate a mixture of odor which can be replaceable of complex biological olfactory systems to smell different type of odorant mixture and concentration of the mixture. It has been used widely for environmental contamination detection (air quality, hazardous gas detection), food quality detection, exhaled breath analysis, etc. It can be used to detect drugs [7]. Electronic noses are arrays of different types of sensors. They can be used to sense different types of gases which posses as biomarker to indicate various diseases.



Fig. 1. VOCs with its related diseases

Various diseases with related exhaled breath

Diabetes: Acetone is a fat burning product and its increase in blood leads to diabetes. The acetone concentration for a healthy person is varied between 0.3 and 1 ppm while increment in concentration from 1.5 ppm to 3.7 ppm leads to diabetic patients [8-10].

Chronic kidney disease: The kidney disease can be identified through NH3 breathing. The concentration of NH3 for healthy person is ~400 to ~1800 ppb while for chronic kidney disease it has been~800 to ~15000 ppb [11].

Blood cholesterol: Isoprene is used to detect the blood cholesterol. The breath analyze developed by Park et al. [12] based on gas chromatography principle. He proposed a ZnO quantum dot (QD) sensor which is helpful in separation of isoprene from mixture of gases then produced electrical signal. The breath analyzer identifies isoprene in the range of 0.40 to 6.2 ppm within 83 s, with high selectivity and sensitivity to trace isoprene in human breath.

Lung cancer: Phillips et. al. (2003) [13] detects lung Cancer through VOCs such as butane; 3-methyl tridecane; 4-methyl octane; 3-methyl hexane; 5-methyl decane. Similarly Chen et. al. (2003) [14] has detected lung cancer using -hexene; hexanol; isoprene; benzene; styrene; decane; undecane; 1 propyl benzene;methyl cyclopentane.

Techniques used for detection

There are various techniques used to develop a breath analyser. Some important techniques are Gas chromatography, Selected ion flow tube-mass spectroscopy, Cavity ring down spectroscopy and E-nose.

Gas Chromatography (GC):

It is widely used method in breath analyser. The basic principle Gas Chromatography is a breath sample is transported in chromatographic column with inert gases such as helium or N₂. The separation of compounds in GC column is performed through boiling points and polarity of the VOCs. Flame ionization detection, mass spectrometry, and ion mobility spectrometry are different methods used in detection for GC. Mass spectrometry is widely used with gas chromatography, called GCMS and the combination was helpful in detecting around 3,000 VOCs with low concentrations.

The Gas chromatography is mainly used for diabities patients beacuse of it high accuracy and sensitive for glucose diagnosis [15]. The drawback of mention technique is sophisticated in use, unportable and expensive.

Selected ion flow tube-mass spectroscopy:

The Selected ion flow tube-mass spectroscopy [16,17] has real time analysis. It is also unportable and expensive with complicated circuitry.

Cavity ringdown specctroscopy:

Cavity ringdown specctroscopy (CRDS) is a technique based on optical spectroscopic. Its working is based on the absorption and scattering of light through the samples [18]. During sample storage and transportation, it suffer from sampling seriously because of loss, decomposition, absorption and reaction of VOCs in breath. The Schematic of CRDS is depicted in figure 2.



Fig. 2. Schematic of CRDS

It is highly responding and sensitive technique but it require high calibration for better results, unporable and expensive [19].

Metaloxide semiconductor based breath analyser:

It is an advanced technique to develop E-nose which is easy to use, portable and highly sensitive. It has arrays of sensors which reacts with definite VOCs. This method is works like a clone of human nose. This technique is portable, easy to handling, high responsive, real time analysis and less costly. The E-nose has been developed mainly using metal oxide based sensor technology.

The metal oxide works on the intraction of gas molecules may be positive or negative charged. The charged molecules converted into electrical properties. connected to the signal conditioning unit. This signal condition unit consists of some active and passive elements. Generally, it will use an operational amplifier, and sensors resistance will be used as a feedback resistor of an operational amplifier. As the Exhaled breath sensor resistance changes, the output voltage also changes, and this output from op-amp will be changed. With the help of multiplexers, all the data from the different sensors can be obtained. This data will be fed into the data acquisition unit. The data acquisition unit will be connected to the PC and the software will analyze the data and give the desired output. Data acquisition software has built-in PCA and SVM algorithms by which data can be easily analyzed.

The E-nose is mainly developed using various metaloxide semiconductor. Commonly used gas sensing materials are Tin Oxide (SnO_2) , Tungsten Oxide (WO_3) , Copper oxide (CuO), Iron oxide (Fe_2O_3) , etc. These oxides are characterized by sensitivity and responce times, but the main disadvantage is its high operating temperature (250 °C to 500 °C) [20,21]. When a volatile organic compound comes in contact with MOX sensing layer. It isolated into charged ions due to which variation takes palce in resistance of sensing film. The change in resistance is depends on the morphology and temperature provide to sensing film.

The different oxides works on different temperature and this temperature will be achived from micro-hoplate. The primary objective is to design low power consumption micro hotplate arrays with a temperature controller. Due to high temperature requirement, MOX sensors need high power consumption, which is an important limitation. To overcome this limitation, different techniques are used for the development of stable tempearture micro-hotplates.

Microelectromechanical system (MEMS):

The MEMS based micro-hotplates consumes low power and miniturize in size. Due to lot of fabrication processes such as wafer cleaning, oxidation in furnace, eatiching, spin coating etc. Its fabrication is costly and complex. The thermal conductivity is also high (150 W/mK) due to which it shows unstability at high temperatures.

Alumina based micro-hotplate:

Thick film technology is used to produce various types of electronic components using the screen printing method. It is also used to produce different types of sensors for gas sensing and chemical application. These sensors have excellent sensing performance and compact design. In the thick film, sensor material generally printed on electrodes, and this electrode printed on a substrate. These thick film sensors considerably cheaper than thin film technology.

Its thermal conductivity is 28 W/mK, and stable on high temperature but it consumes high power and structuring is very typical on alumina substrate.

LTCC based micro-hotplate:

Low temperature cofired ceramic(LTCC) technique used to fabricate gas sensors and useful technology for circuit and package fabrication. These sensors have excellent performance because of its electrical characteristics and thick film pastes compatibility. It uses a multi-layer fabrication process and possible to manufacture 3D structures [24]. This technology is very attractive due to their packaging as they have the capability to prepare channels, cavities, diaphragms, passive component integration, etc [25]. This technology used in a wide range of applications such as gas sensors, fluid mixers, bandpass filters, strip antenna, etc. LTCC technology offers a lot of advantages that can be utilized in the production of various kinds of electronic noses in one module [24,26]. LTCC technology also enables the fabrication of threedimensional (3D) structures which is especially desirable in the case of electronic nose applications and micro-fluidics applications.

The comparision of LTCC and alumina micro-heaters has been indicated by kulhari *L et. al.* 2019 as shown in figure 3. Here characterization has been performed for same structure of alumina and LTCC substrate with differ ent thicknesses of LTCC substrate and analysed that LTCC consumes low power in comparision to alumina.



Fig.3 (a) Tem (°C) vs applied voltage (V) & (b) Tem (°C) vs power consumption (W) of LTCC/alumina micro-heaters [27]

The micoheaters developed using LTCC substrate are miniturize in size. The LTCC based micro-heaters has been successfully demonstrated for gas sensor applications [28-30].

Conclusion:

Developed micro hotplate arrays will be Characterized and compared with the simulated results. Characterization would involve various analytical tests to extract information related to the surface morphology, temperature distribution, and current-carrying mechanisms of the micro-hotplate. This would provide a feedback loop to fabricate better and improved micro- hotplate. The exhaled breath sensing material such as Tin(IV) Oxide (SnO₂), Copper (II) oxide (CuO), Zinc oxide (ZnO), Titanium dioxide (TiO₂), Indium (III) oxide (In₂O₃), and Iron (III) oxide (Fe₂O₃), etc shall be deposited by different methods such as thick film paste formation, sol-gel technology, and thin-film coating. The main purpose is to develop a fast and scientific determination of volatile organic compounds in the exhaled breath for real-time measurements and low costs. The developed biomarker will focuses to provide proper information on disease or asthma, diabetes, and lung cancer or the effects of treatment.

The LTCC-based MOX sensors are better E-nose for VOCs. The LTCC based E- Nose can be easily detect different types of diseases such as lung cancer, diabetics, by analyzing the exhaled breath of a patient. It will be a portable device with long life and provede stable output.

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REFERENCES

- Hsu, C. M., Liao, W. Y., Luo, C. H., & Chou, T. C. (2007) The 2.4 GHz biotelemetry chip for healthcare monitoring system, *Sensors and Actuators A: Physical*, 139, No. 1-2, 245-251.
- [2] Turner, C., Španěl, P., & Smith, D. (2005). A longitudinal study of breath isoprene in healthy volunteers using selected ion flow tube mass spectrometry (SIFT-MS). *Physiological Measurement*, 27(1), 13.
- [3] Saidi, T., Zaim, O., Moufid, M., El Bari, N., Ionescu, R., & Bouchikhi, B. (2018). Exhaled breath analysis using electronic nose and gas chromatography–mass spectrometry for noninvasive diagnosis of chronic kidney disease, diabetes mellitus and healthy subjects. *Sensors and Actuators B: Chemical*, 257, 178-188.
- [4] Amann, A., & Smith, D. (Eds.). (2013). Volatile biomarkers: non-invasive diagnosis in physiology and medicine. Newnes.
- [5] D'Amico, A., Pennazza, G., Santonico, M., Martinelli, E., Roscioni, C., Galluccio, G., ... & Di Natale, C. (2010). An investigation on electronic nose diagnosis of lung cancer. *Lung cancer*, 68(2), 170-176.
- [6] Dragonieri, S., Schot, R., Mertens, B. J., Le Cessie, S., Gauw, S. A., Spanevello, A., ... & Bel, E. H. (2007). An electronic nose in the discrimination of patients with asthma and controls. *Journal of Allergy and Clinical Immunology*, 120(4), 856-862.
- [7] Wu, C. C., Chiu, S. W., & Tang, K. T. (2019). An Electronic Nose System for Rapid Detection of Ketamine Smoke. *IEEE Sensors Letters*, 3(8), 1-4.
- [8] Deng, C., Zhang, J., Yu, X., Zhang, W., & Zhang, X. (2004). Determination of acetone in human breath by gas chromatography–mass spectrometry and solid-phase microextraction with on-fiber derivatization. *Journal of Chromatography B*, 810(2), 269-275.
- [9] Chakraborty, S., Banerjee, D., Ray, I., & Sen, A. (2008). Detection of biomarker in breath: A step towards noninvasive diabetes monitoring. *Current Science*, 237-242.
- [10]Nasution, T. I., Nainggolan, I., Hutagalung, S. D., Ahmad, K. R., & Ahmad, Z. A. (2013). The sensing mechanism and detection of low concentration acetone using chitosan-based sensors. Sensors and Actuators B: Chemical, 177, 522-528.
- [11]Davies, S., Spanel, P., & Smith, D. (1997). Quantitative analysis of ammonia on the breath of patients in end-stage renal failure. *Kidney international*, 52(1), 223-228.
- [12]Park, Y., Yoo, R., ryull Park, S., Lee, J. H., Jung, H., Lee, H. S., & Lee, W. (2019). Highly sensitive and selective isoprene

sensing performance of ZnO quantum dots for a breath analyzer. Sensors and Actuators B: Chemical, 290, 258-266.

- [13]Phillips, M., Cataneo, R. N., Cummin, A. R., Gagliardi, A. J., Gleeson, K., Greenberg, J., ... & Rom, W. N. (2003). Detection of lung cancer with volatile markers in the breath. *Chest*, *123*(6), 2115-2123.
- [14]Chen, X., Xu, F., Wang, Y., Pan, Y., Lu, D., Wang, P., & Zhang, W. (2007). A study of the volatile organic compounds exhaled by lung cancer cells in vitro for breath diagnosis. *Cancer: Interdisciplinary International Journal of the American Cancer Society*, 110(4), 835-844.
- [15]Yan, K., Zhang, D., Wu, D., Wei, H., & Lu, G. (2014). Design of a breath analysis system for diabetes screening and blood glucose level prediction. *IEEE transactions on biomedical engineering*, 61(11), 2787-2795.
- [16]Moorhead, K., Lee, D., Chase, J. G., Moot, A., Ledingham, K., Scotter, J., ... & Endre, Z. (2007, August). Classification algorithms for SIFT-MS medical diagnosis. In 2007 29th Annual International Conference of the IEEE Engineering in Medicine and Biology Society (pp. 5178-5181). IEEE.
- [17]Smith, D., & Španěl, P. (2005). Selected ion flow tube mass spectrometry (SIFT-MS) for on-line trace gas analysis. *Mass* spectrometry reviews, 24(5), 661-700.
- [18] Wang, C., Mbi, A., & Shepherd, M. (2009). A study on breath acetone in diabetic patients using a cavity ringdown breath analyzer: exploring correlations of breath acetone with blood glucose and glycohemoglobin A1C. *IEEE Sensors Journal*, 10(1), 54-63.
- [19]áP MILLER, G., & áB WINSTEAD, C. (1997). Inductively coupled plasma cavity ringdown spectrometry. *Journal of Analytical Atomic Spectrometry*, 12(9), 907-912.
- [20]Blatt, R., Bonarini, A., Calabro, E., Della Torre, M., Matteucci, M., & Pastorino, U. (2007, August). Lung cancer identification by an electronic nose based on an array of MOS sensors. In 2007 International Joint Conference on Neural Networks (pp. 1423-1428). IEEE.

- [21]Wang, C., Yin, L., Zhang, L., Xiang, D., & Gao, R. (2010). Metal oxide gas sensors: sensitivity and influencing factors. *sensors*, 10(3), 2088-2106.
- [22]Lee, J., Choi, N. J., Lee, H. K., Kim, J., Lim, S. Y., Kwon, J. Y., ... & Yoo, D. J. (2017). Low power consumption solid electrochemical-type micro CO2 gas sensor. *Sensors and Actuators B: Chemical*, 248, 957-960.
- [23]Jain, Y. K., & Khanna, V. K. (2007, December). Thick film, LTCC or silicon microhotplate for gas sensor and other applications. In 2007 International Workshop on Physics of Semiconductor Devices (pp. 714-717). IEEE.
- [24]Kulhari, L., & Khanna, P. K. (2018). Design, simulation and fabrication of LTCC-based microhotplate for gas sensor applications. *Microsystem Technologies*, 24(5), 2169-2175.
- [25]Yan, Y. Z., Lu, H. X., & Tang, X. P. (2015). Fabrication of typical 3D structure on ltcc for microsystem.
- [26]Rydosz, A. (2018). Sensors for enhanced detection of acetone as a potential tool for noninvasive diabetes monitoring. Sensors, 18(7), 2298.
- [27]Kulhari, L., Chandran, A., Ray, K., & Khanna, P. K. (2019). Design, fabrication and characterization of LTCC microhotplates for gas-sensing application. *Microelectronics International.*
- [28]Kulhari, L., Ray, K., Paptan, A., Suri, N., & Khanna, P. K. (2020). Development of LTCC micro-hotplate with PTC temperature sensor for gas-sensing applications. *International Journal of Applied Ceramic Technology*, *17*(3), 1430-1439.
- [29]Kulhari, L., Ray, K., Suri, N., & Khanna, P. K. (2020). Detection and characterization of CO gas using LTCC microhotplates. Sādhanā, 45(1), 1-6.
- [30]Rettig, F., & Moos, R. (2004). Ceramic meso hot-plates for gas sensors. Sensors and Actuators B: Chemical, 103(1-2), 91-97.